

ORIENTAL JOURNAL OF CHEMISTRY

An International Open Free Access, Peer Reviewed Research Journal

www.orientjchem.org

ISSN: 0970-020 X CODEN: OJCHEG 2018, Vol. 34, No.(4): Pg. 2180-2186

An Efficient Electrochemical Approach for Characterization of the Interface Strength of Nano Titania-Silica (TS) Composite **Coating on Titanium Implants**

SUJA MATHAI

Department of Chemistry, Mar Ivanios College, Nalanchira, Thiruvananthapuram, Kerala-695 015, India. *Corresponding author E-mail: sujamathaikunnath@gmail.com

http://dx.doi.org/10.13005/ojc/3404060

(Received: January 16, 2018; Accepted: July 31, 2018)

ABSTRACT

The thermal decomposition process developed in the present work is a viable technique for the formation of a nano (TiO₂-SiO₂) composite coating on Titanium substrate. The electrochemical experiments revealed that the developed coatings had high degradation resistance characteristics and high biomimetic growth characteristics. There was no degradation on the coating even when it was subjected to different extent of electrochemical polarization and anodic current impression. The biomimetic growth studies of these coatings were carried out without any alkaline treatment. Surface and topographical analysis including SEM and AFM were also carried after biomimetic growth. The results of elemental analysis of the SBF solution and electrochemical characterization carried out at different stages revealed that there was efficient apatite growth even without pre-alkaline treatment.

Keywords: Titania-silica composite coating, Titanium implants, Biomimetic growth, Electrochemical characterization.

INTRODUCTION

The magnitude of molecular and cellular events at the tissue-implant interface are controlled by the bioactivity and topography of the biomaterial surface.1 Bioactive nano-structured coatings applied on an orthopaedic implant can mimics the properties of a physiological bone.^{1,2} In the work of Liu X et al., it was mentioned that CaP precipitation can be more easily induced by a nano TiO₂ surface than a conventional TiO₂ surface.³ The hydroxyapatite (Hap) crystals thus formed on these bioactive coatings in body environment has a crystallographic matches with that of bone apatite crystals.⁴ These nano TiO, particles can be coated on to metallic implants by plasma spraying. In plasma-sprayed coatings, difficulties such as maintaining phase purity and mechanical strength in vivo, have been encountered.^{5,6} It was reported that, a nano TiO, pre layered-HAp coating showed more adhesion and bioactivity than the single HAp coating on Ti in simulated body fluid (SBF).



CODED This is an Open Access article licensed under a Creative Commons Attribution-Non Commercial-Share Alike NC SA Non Commercial use, distribution and reproduction in any medium, provided the original work is properly cited.

The present study focuses on the development of a nano TS composite coating by a comparatively low temperature thermal decomposition process and its further evaluations under different aggressive and simulated conditions to establish the mechanical, biochemical and biological characteristics including non-cytotoxicity. There was a view of using the implants without any alkaline treatment before biomimetic apatite growth study, so that high bone bonding could be predicted.

EXPERIMENTAL

The SiO₂ nano powders were added on to TiCl,/isopropanol solutions and its composition was optimized. A thin layer of the TiCl₄/isopropanol+SiO₂ was applied on a pretreated Ti substrate and was subjected to continuous heating in a furnace at 500°C for an hour.⁶ Bio-electrochemical behaviour of these TS composite coatings were compared with that of the TiO₂ coatings developed by the same process. A Vicker's microhardness indenter used to measure the microhardness of these coatings. A maximum load was applied till the coating became flake off. The degradation characteristics of the developed coatings on Ti in 9% NaCl solution, i.e., 9 times concentration of normal physiological solution and in Kokubo's simulated body fluid (SBF)8 under normal and accelerated conditions, i.e., applying external current densities, were studied. Cyclic polarization study was also done to assess the coating stability. The degradation characteristics of the coatings were further analyzed by EIS measurement. Surface morphology of the coatings was analyzed by SEM and optical microscopy. The chemical analysis of the SBF solutions before and after polarization studies were done by ICP-AES.

The biomimetic growth characteristics of the coatings were studied by immersing in Kokubo's SBF for 2 weeks at 36.5° C. The topographic analysis of the coatings was carried out by AFM and SEM techniques. The elemental analysis was done by EDS. EIS studies were also carried out to compare the apatite growth characteristics of both TiO₂ and TS composite coatings on Ti.

An *in vitro* cytotoxicity test was performed for both TiO_2 and TS composite coatings on Ti using

direct contact method as per ISO 10993-5. An ultra high molecular weight poly ethylene (UHMWPE) and poly vinyl chloride (PVC) were used as negative and positive controls respectively. The test samples, negative controls were placed on a subconfluent monolayer of L-929 mouse fibroblast cells. After incubation of the cells with test samples at 37 + 2°C for 24 + 1 h, the cell culture was examined microscopically for any cellular response around test samples.

RESULTS AND DISCUSSION

The most important property required for a composite coating on a metallic implant for orthopaedic applications is its mechanical stability. Fig. 1 shows the micro-hardness data of both TiO_2 and TS composite coatings under various applied loads.



Fig. 1. Microhardness of TiO_2 (\square) and TS (\square) composite coatings on Ti for various applied loads.

The micro-hardness values were found increased with increase in the applied loads. The nano TS composite coating exhibited higher micro-hardness values than the nano TiO_2 coating throughout the tests under all the different loads applied. These coatings were stable up to an applied load of 50 gm. The enhanced mechanical stability of the TS composites were due to the formation of a network layer of Ti-O-Si linkages on the surface of Ti and thereby has an increase in bonding strength of the TiO₂ coating with an optimum amount of silica. The nano TiO_2 dispersed in a SiO₂ matrix have tetrahedral structure, which can serve as active sites for further apatite formation⁹.

The composite coatings applied on metallic implants used for load bearing applications must have adequate adhesive strength at their interfaces.¹⁰ The potential values of both the TiO₂ and TS composite coatings on Ti even after subjecting to a current density of 5mA/cm² for 4 h in 9% NaCl and also in SBF solutions were found to be remained constant during the entire period. There was a minute shift in the potential from the initial value was observed, i.e., +1.8V. There was no surface blemishing or detachment took place on both the TiO₂ and TS composite coatings even after applying a current density of 5mA/cm² for 4 hours. This was revealed from the optical micrographs as shown in Figure 2.



Fig. 2. Optical micrographs of TiO_2 and TS composite coatings on Ti (a) before applying current, (b) after applying a current density of 5mA/cm² for 4 h in SBF solution and (c) after applying a current density of 5mA/cm² for 4 h in 9% NaCl solution

ICP-AES analysis of the 9% NaCl solution, in which degradation study was carried out also confirmed these results that there was 0.00 results obtained for the elemental determination of Ti and Si. OCP variation with time of nano TiO_2 and TS composite coatings on Ti in 9% NaCl at 36.5°C was carried under a current density of 5mA/cm² for 4 hours. Fig. 3 shows that the initial and final surface potentials remained constant.



Fig. 3. OCP variation with time of nano TiO2 (O) and TS composite (Δ) coatings on Ti in 9% NaCl at 36.5°C

EIS results before and after degradation studies of the coatings is given in

Table 1. The resistance values of both the outer porous layer got reduced but not to a considerable extend and therefore a corresponding increase in the capacitance value was observed. ICP-AES results showed that there were no Ti and Si in the physiological solution even after accelerated tests.

Table 1: The electrochemical impedance parameters nano TiO2 and TS composite coatings on Tisubstrate before and after immersion in 9% NaCI

SI. No	Composite coating on Ti substrate	$R_{_{pL}}$ Ohm	$C_{_{pL}} \mu F$	R _{₅∟} kOhm	$\rm C_{_{bL}}pF$	n	Chi-square
(a)	Before immersion in 9% NaCl						
1	TiO ₂	24.2	34.8	0.15	14.24	1.23	9.34
2	TS	44.8	39.4	3.81	22.29	1.22	9.44
(b)	After immersion in 9% NaCl						
3	TiO ₂	22.2	34.8	0.14	1.00	1.26	9.69
4	TS	43.6	54.1	3.66	1.00	1.26	9.69

The cyclic polarization curves of both TiO_2 and TS composite coatings are presented in Fig. 4. No film breakdown was observed on the samples. After cyclic polarization, both the coatings were found adherent to the substrate. Semi-quantitative analysis by ICP-AES was performed with the 0.9 % NaCl solution in which the cyclic polarization was conducted. No Ti or Si was detected in the solution revealing that there was no degradation of the coating occurred during polarization studies. The native oxide layer of nanometer thickness that already exists on the Ti substrate generates a strong mechanical bond between the TiO_2 and SiO_2 particles at the interface of the coating.



Fig. 4. Cyclic polarization curves of (a) TiO_2 and (b) TS composite coatings

Figure 5 shows the AFM image and the line profiles of both the TiO_2 and TS composite coatings prior to immersion in SBF solution describes the surface topography. The line profiles of both TiO_2 and TS coatings are found smaller and thinner, showing much smoother surface structures. Rmax (maximum roughness) values obtained for these coatings were 180 and 550 nms respectively.

Figure 6 shows the AFM image and the line profiles of the nano TiO_2 and TS composite coatings after biomimetic growth in SBF at pH:7.4 and 36.5°C for 14 days. Rmax values got decreased for both the TiO₂ and TS composite coatings due to the formation of crystals of HAp on their surface. The corresponding SEM pictures shown in Fig. 7 also exhibit the presence of white precipitates of HAp on its surface.

The apatite growth on the surface of both TiO_2 and TS composite coatings were also confirmed by EIS results as shown in Table 2. After biomimetic growth the RpL and RbL values got increased,

revealing that the increased resistance was offered by the apatite grown on its surface.



Fig. 5. AFM - the three dimensional and two dimensional images (including line scan) of (a) TiO₂ and (b) TS composite coatings on Ti



Fig. 6. AFM - the three dimensional and two dimensional images (including line scan) of (a) TiO₂ and (b) TS composite coatings on Ti after immersion in Kokubo's SBF for 14 days



Fig. 7. SEM micrographs of (a) TiO₂ and (b) TS composite coatings on Ti after biomimetic growth in Kokubo's SBF for 14 days

Table 2: The electrochemical impedance parameters nano TiO2 and TS composite coatings on Ti substrate before and after biomimetic growth in Kokubo's SBF for 14 days.

SI. No	Composite coating on Ti substrate	$R_{_{pL}}Ohm$	$C_{pL}nF$	R _{ь∟} kOhm	$C_{_{bL}}\mu F$	n	Chi-square
(a)	Before biomimetic growth in SBF						
1	TiO ₂	16.24	104.1	1.72	76.00	1.25	11.59
2	TS	18.94	34.8	2.14	64.24	1.262	9.69
(b)	After biomimetic growth in SBF						
3	TiO ₂	21.91	77.2	3.94	51.20	1.02	12.56
4	TS	26.11	29.59	4.83	42.3	1.01	13.3



Fig. 8. Nyquist plots of (a) TiO₂ coating (O; before and •; after) and (b) TS composite coating (O; before and •; after) biomimetic growth in Kokubo's SBF for 14 days

Figure 8 shows the Nyquist plots of the nano TiO₂ and TS composite coatings after biomimetic growth in SBF solution at 36.5°C and pH: 7.4 for 14 days. It can also be inferred that more apatite could be induced on the surface due to long term immersion in SBF solution. The TS could be charged negatively in a solution with a physiological pH:7.4 and hence attract the positively charged Ca²⁺ ions and then PO₄³⁻ groups in the SBF favoring apatite growth. Apatite nuclei are initiated once, the super saturation rises over the critical level necessary for heterogeneous nucleation of apatite.¹¹⁻¹⁵

The microstructure and crystallinity of TiO_2 or SiO_2 may be the important factors influencing the nucleation of apatite on the surface. 16 XRD patterns of the TiO_2 and TS composite coating is shown in Fig. 9. Compared with the standard cards of JCPDS, the major peaks appeared at $2^{\circ}=37^{\circ}$, 48° and 55° are the peaks of anatase TiO₂. The XRD pattern of the TiO₂ and TS composite coatings formed after biomimetic growth in SBF is shown in Fig. 10. The peaks appeared at $2^{\circ}=25^{\circ}$, 40° , 45° , and 55° are the characteristic peaks of HAp. The intensity of the HAp peaks got increased and also more peaks of HAp for the TS composite coatings, which shows its enhanced bioactivity



Fig. 9. XRD patterns of (a) TiO_2 and (b) TS composite coatings

The developed nano TiO₂ and TS crystalline particles have higher surface charge densities¹⁷ and readily absorb molecules or ions onto their surfaces in SBF in order to decrease the total free energy and to become more stable.³ It can be further demonstrated by thermodynamic analysis that the interfacial tension also diminishes due to decrease in particle size.¹⁸ There is also a crystallographic matching between the apatite (0001) plane and the anatase (110) plane.¹⁹ This may lead to higher apatite forming ability of the nano-sized anatase form of the TiO₂ particles. After *in vitro* cytotoxicity tests, from Fig. 11 it was found that fibroblast cells had grown over the surface of the TS composite coating on Ti. The fibroblast cells retained its spindle shapes and no rupturing was occurred during incubation of the cells with test samples for 24 + 1 hours.



Fig. 10. XRD patterns of (a) TiO₂ and (b) TS composite coatings after biomimetic growth in Kokubo's SBF for 14 days

Table 3 shows the qualitative evaluation of in vitro cytotoxicity test. Cellular responses were scored as 0, 1, 2, and 3 according to non-cytotoxic, mildly cytotoxic, moderately cytotoxic and severely cytotoxic. The TS coated substrates were found to be non-cytotoxic to the fibroblast cells. Negative controls gave non-cytotxic response while the positive controls gave severely cytotoxic response as expected.

CONCLUSION

The thermal decomposition process developed in the present work is a viable technique for the formation of TS composite coatings on Ti substrate as a stable network of TS oxide layer is formed during the process. High mechanical stability of the TS composite coating was revealed by its hardness under various applied loads and it could withstand against an applied load up to 25 g. There was no degradation on the coating even when it was subjected to different extent of electrochemical polarization and anodic current impression. There were no detachment or decohesion of the coating



Fig. 11. Photograph of fibroblast cells around nano TS composite coated Ti

Table 3: The results of Qualitative evaluation of in vitro cytotoxicity test

SI. No	. Sample Cyto o s	otox cale	icity Ə	Interpretation
1	Negative control	0		Non-cytotoxic
2	Positive control	3	S	everely cytotoxic
3	Sample (TS coated Ti)	0		Non-cytotoxic

after polarization. There was no elemental detection of Ti or Si in the physiological solutions after the polarization studies revealing a very good adherence of the TS coating. Hence the present electrochemical approach is found to be worth to analyze the adhesion strength.

The results of surface and topographical analysis including SEM and AFM, and elemental analysis of SBF solution revealed an appreciable biomimetic growth character even without any alkaline pre-treatment. These inferences were further supported by the increased resistance values obtained during electrochemical impedance studies. The non-cytotoxic behavior of the TS coated substrate to fibroblasts cells revealed cytocompatibility. The present nano TiO_2 and TS composite coatings developed on Ti implants by thermal decomposition process can withstand under aggressive body environment conditions and has very good cytocompatibility.

ACKNOWLEDGEMENT

The author acknowledges the financial support from UGC, New-Delhi.

REFERENCES

- 1. Webster, T. J.; Siegel, R. W.; Bizios, R. *Biomaterials.*, **1999**, *20*, 1221.
- Ohtsuki, P. Li, C.; Kokubo, T.; Nakanishi, K.; Soga, N.; Groot, de. K. *J. Biomed. Mater. Res.*, 1994, *7*, 28.
- Liu, X.; Zhao, X.; Fu, R.K.Y.; Ho, J.R.Y.; Ding, C.; Chu, K.P. *Biomaterials.*, 2005, 26, 6143.
- Areva, S.; Aaritalo, V.; Tuusa, S.; Jokinen, M.; Linden, M.; Peltola, T. *J Mater. Sci. Mater. Med.*, 2007, *18*, 1633.
- Milella, E.; Cosentino, F.; Licciulli, A.; Massaro, C. *Biomaterials.*, 2001, 22, 1425.
- 6. Shibli, S.M.A.; Mathai, S. *J. Mater. Sci. Mater. Med.*, **2008**, *19*, 2971.
- Lin, C.M.; Yen, S.K. J. Mater. Sci. Mater. Med., 2005, 16, 889.
- Kokubo, T.; Takadama, H. *Biomaterials.*, 2006, 27, 2907.
- Sun, D.; Huang, Y.; Han, B.; Yang, G. Langmuir., 2006, 22, 4793.
- 10. Morks, M.F. *J. Mech. Behav. of Biomed. Mater.*, **2008**, *1*, 105.
- 11. Jokinen, M.; Patsi, M.; Rahiala, H.; Peltola, T.;

Ritala, M.; Rosenholm, J. B. *J. Biomed. Mater. Res.*, **1998**, *42*, 295.

- 12. Li, P.; Kangasniemi, I.; Groot, de, K. *J. Am. Ceram. Soc.*, **1994**, *77*, 1307.
- Corbridge, D.E.C. The structural chemistry of phosphorus. Elsevier, Amsterdam-London –New York., **1984**.
- Shou, G.; Dong, L.; Liu, Z.; Cheng, K.; Weng,
 W. ACS Biomater. Sci. & Engg., 2017, 6, 875.
- Guo, Y.; Tan, Y.; Liu, Y.; Liu, S.; Zhou, R.; Tang, H. *Mater. Sci. & Engg.*, C 2017, *80*, 197.
- 16. Ishizawa, H.; Ogino, M. *J. Biomed. Mater. Res.*, **1995**, *29*, 1071.
- Vayssieres, L.; Chaneac, C.; Trone, E.; Joliver, J.P.; *J. Colloid Interface Sci.*, **1998**, *205*, 205.
- Zhang, H.; Penn, R. L.; Hamers, R. J.; Banfield, J. F. *J. Phys. Chem.*, B **1999**, *103*, 4656.
- Uchida, M.; Kim, H.M.; Kokubo, T.; Fujibayashi, S.; Nakamura, T. *J. Biomed. Mater. Res.*, Part B, **2003**, *64*A, 164.