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# Composite Film of Chitosan Loaded Norfloxacin With Improved Flexibility and Antibacterial Activity for Wound Dressing Application

NOR JANNAH MOHD SEBRI<sup>1</sup> and KHAIRUL ANUAR MAT AMIN<sup>1,2</sup>

<sup>1</sup>School of Fundamental Science, Universiti Malaysia Terengganu, 21030, Kuala Terengganu, Malaysia.
<sup>2</sup>Institute of Marine Biotechnology, University Malaysia Terengganu, 21030 Terengganu, Malaysia.
\*Corresponding author E-mail: kerol@umt.edu.my

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## ABSTRACT

This research develops chitosan film incorporated norfloxacin (CH-NOR) designed to combat the infection of bacteria around the wound area. Inclusion of norfloxacin increased the strain-atbreak or flexibility of the film. Swelling behavior and water vapor transmission rates (WVTRs) values are improved and optimum for CH-NOR1.0 film at 524  $\pm$  65 % and 1916  $\pm$  78 g m<sup>2</sup> d<sup>-1</sup>, respectively. *In-vitro* cell studies show that the present of norfloxacin in CH film gradually decreased the number of human dermal fibroblast cell (CRL2522, ATCC) after incubated for 72 hours. In-contrast, antibacterial activities of CH-NOR films exhibit strong inhibition zones against *Gram-positive (Staphylococcus aureus* and *Bacillus cereus*) and *Gram-negative (Escherichia coli* and *Klebsiella pneumoniae*) bacteria.

Keywords: Chitosan, Norfloxacin, Film, Biomaterials, Wound dressing.

# INTRODUCTION

Chitosan (CH) is an attractive polymer to be considered for medical applications as they are biocompatible and biodegradable. It is a linear cationic polysaccharide, and one of the most abundant polysaccharides occurring in nature. It is structurally similar to the extracellular matrix component glycosaminoglycans (GAGs) and has been utilized in the field of biomedicine as dressing materials<sup>1</sup>, scaffolds<sup>2</sup> and pharmaceuticals delivery agent<sup>3</sup> by promoting bone cell division as well as bone growth. It is also used in other applications such as contact lenses<sup>4</sup>, anticoagulant<sup>5</sup> and anticancer substances<sup>6</sup>. The ease of CH fabrication to form variety of products such as gels, scaffolds, films, filaments, powders, sponges, composite or as nanofibers further accelerates the usability of this material<sup>7</sup>.

Various studies have been reported on developing CH film as dressing products by incorporating difference therapeutic agents or specifically antibiotic agents. Sezer and coworkers introduced fucoidan into porous CH film to investigate its suitability for the treatment of dermal burns on rabbits8. The results show that fucoidan-CH film has the fastest closure of wounds after 14 days compared with other treatments. Many other therapeutic agents have been reported in CH films such as amikacin and dapromycin<sup>9</sup>, ciprofloxacin hydrochloride<sup>10</sup> and ornidazole<sup>11</sup>. Antibiotics derived from fluoroquinolone groups are among the rapid growing class of antimicrobial agents that has proved the effectiveness in treatment of bacterial infection<sup>12</sup>. All the fluoroquinolone groups have a fluorine at position 6 of a naphthyridine ring and few of them are levofloxacin, gatifloxacin, lemofloxacin and norfloxacin with different functional groups  $(R_1, R_2, R_3 \text{ and } R_4)^{13}$ . Norfloxacin has a broad spectrum of activity against Gram-positive and Gram-negative bacteria especially aerobes with limited activity against anaerobes<sup>14</sup>. It is also effective in treatments of a wide range of clinical infections including the urinary tract,<sup>15</sup> and liver cirrhosis<sup>16</sup>. Having said this norfloxacin can combat lot of bacteria, limited studies have been discussed on the effect of norfloxacin in biopolymer composite film to be applied as wound dressing materials. Chitosan sponges with norfloxacin have been examined and show excellent antibacterial activity proportional to the release rate<sup>17</sup>. Other study reported on chitosan microsphere loaded norfloxacin with improved antibacterial effect<sup>18</sup>. Different biopolymer, i.e. polyvinyl alcohol (PVA) film containing norfloxacin (5% w/w) also show comparable in-vitro performances and healing effects to commercial silver sulfadiazine (1% w/w) cream<sup>19</sup>.

In this study, we highlighted the properties of CH film loaded with norfloxacin (CH-NOR) as an effective material to combat the bacteria. Not limited to that, the mechanical performances, physical properties such as swelling capability and water vapor transmission rates of the CH-NOR film are examined to optimize the properties of the materials. The cell viability and cell proliferation tests are also carried out to study the biocompatibility of the CH-NOR films involved human skin fibroblast cell (CRL2522, American Type Tissue Collection), while the antibacterial activities of the samples were assessed via *in-vitro* qualitative study against *Gram-positive* and *Gram-negative* bacteria.

## MATERIALS AND METHODS

#### **Materials**

Chitosan (CH: medium molecular weight, 75% degree of deacetylation (DD), viscosity  $\approx$  453 cP) and glacial acetic acid were obtained from Sigma Aldrich, St Louis, MO while penicillin G-P10 was obtained from Oxoid, England. Norfloxacin was obtained from Fluka, Malaysia. All materials were used as received without further purification.

## Preparation of chitosan with norfloxacin

Chitosan (CH) solution was prepared by dissolving 2% w/w in acetic acid (0.1 M) and heated for 2 h at 70 °C. Glycerin (30%, w/w) was added into the CH solution followed by norfloxacin (0.1, 1.0 and 5.0% w/w) henceforth referred to as CH-NOR0.1, CH-NOR1.0 and CH-NOR5.0, respectively. The CH solutions were then cooled in ambient temperature for 24 h to let the debris and extraneous matter precipitated at the bottom of the beaker, forming a clear yellowish solution. The CH solutions were then poured onto an acrylic plate and dried in oven at 50 °C for 24 hours.

## Characterization ATR-FTIR

ATR-FTIR spectra were collected using a Perkin Elmer Spectrum 100 FTIR spectrophotometer with PIKE Miracle ATR accessory (single-bounce beam path, 45 ° incident angle, 16 scans, and 4 cm-<sup>1</sup> resolution). All spectra were corrected by the Perkin Elmer Spectrum 100 software.

#### **Mechanical properties**

Tensile strength measurements were obtained using an Instron Universal Testing machine (model 3366) with  $\pm$  10 kN grips and cross-speed set at 10 mm/min according to ASTM standard method D 882-01. All films were cut to 20 mm x 60 mm, and film's thickness was measured using a Mitutoyo hand-held micrometre. Young's modulus (E), tensile

strength (TS), and toughness (T) were calculated from the slope of the linear part of the stress-strain curve, the maximum stress, and by integrating the area under the stress-strain curve, respectively. A minimum of three independent measurements were obtained per sample.

## **Swelling Analysis**

The swelling test was carried out by immersing dried films (20 mm x 20 mm) in phosphate buffer solution (pH 7) in water bath (37  $\pm$  0.5 °C). The samples were then removed after 24 h, lightly blotted with a wet filter paper to expel surface solution prior to measuring the weight. The test was repeated triplicates for each ratio. Finally, the swelling degree was then determined from the equilibrium-swelling ratio:

Swelling Degree, SD (%) =  $(M_{w} - M_{d})/M_{d}$ 

where  $M_w$  = Weight of swollen sample and  $M_d$  = Weight of dry sample

#### Water Vapor Transmission Rate

The water vapor transmission rate (WVTR) test was carried out using the method adapted from the previous study <sup>20</sup>. Briefly, films with dimension of 30 mm x 30 mm was cut and put as a cap of a glass vial with a diameter 16 mm containing 10 mL distilled water, followed by the system being weighed and recorded. Each ratio of samples was made into triplicates and stored in humidity chamber for 24 h at T= 37.5 °C and relative humidity of 60 % ± 5. The value for WVTR (g m<sup>-2</sup> d<sup>-1</sup>) was calculated as follows;

$$WVTR = (W_i - W_f)/(A)$$

where A = area of the vial opening,  $W_i$  = initial weight of the system and  $W_f$  = final weight of the system.

## Cell Study

## Routine cell-culture

The cultivation of normal human skin fibroblast cells (CRL-2522, ATCC) was prepared by using the Eagle's Minimum Essential Medium (EMEM, ATCC, USA) with 10 % (v/v) fetal bovine serum (FBS, Sigma Aldrich, USA) and 1% (v/v) antibiotic (Penicillin/ Streptomycin, Sciencell, USA). In addition, the cells were cultured at 37 °C in a humidified 5 %  $CO_2$  atmosphere and were subcultured every three days as established protocols and harvested at 60-80 % confluence.

#### **Cell Viability**

The chitosan films (diameter ~6mm) were placed into the 96-well culture plates (Nunc, Germany) containing EMEM medium prior to sterilize in a laminar airflow chamber under UV radiation for 20 minutes. The CH films were sterilized in a laminar airflow chamber under UV radiation for 20 min. The next step followed with having three replicates used for each type of samples. The CRL2522 cells (5000 cells/ well) were seeded into wells containing samples and cultured at 37 °C in 5 % CO<sub>2</sub> atmosphere. Tissue culture polystyrene plates (TCPP) were used as a control, and after 24 h, 48 h, and 72 h of incubation, the cell viability were observed by using an Olympus TH4-200 microscope equipped with an Olympus U-RFL-T UV pack stained with calcein-AM.

## **Cell Proliferation**

Cell proliferations were quantified by using CellTiter 96 aqueous one solution assay (Promega, USA), which contained tetrazolium compound [3-(4, 5-dimethylthiazol-2-yl)-5-(3- carboxymethoxyphenyl)-2-(4-sulfophenyl)-2H tetrazolium), inner salts; MTS (a)] with electroncoupling reagent (phenazineethosulfate). Prior to the addition of the assay solution (20 µL in each wells), the media in all wells that contained samples, except for the positive control, were replaced with fresh media and later incubated for 3 h at 37 °C in an atmosphere containing 5% CO<sub>2</sub>. Then, 100 µL of the inoculants were transferred into new wells and the absorbance at 490 nm was measured by using a microplate reader (Multiskan Ascent 96/384, USA). The absorbance readings were converted to cell number using calibration curves.

#### **Antibacterial Study**

Gram-positive (Staphylococcus aureus & Bacillus cereus) and Gram-negative (Escherichia coli & K. pneumoniae) bacterial suspensions were used for the antibacterial assay. Mueller-Hinton (MH, Difco, Malaysia) agar was used for the growth of both bacterial types. Each Gram-positive and Gram-negative bacteria suspension was evenly spread on the solid MH agar and dried in a laminar flow air chamber. The samples (diameter ~ 6 mm) were adhered on the agar surface. The LB agar with the CH film samples was incubated at 37°C for 24 hours. The presence of any clear zone around the film on the LB agar was recorded as an indication of inhibition against the *S. aureus, B. cereus, E. coli* and *K. pneumoniae*.

## **RESULTS AND DISCUSSIONS**

# **ATR-FTIR**

Fig. 1 shows the ATR-FTIR spectra of chitosan (CH) films incorporated with norfloxacin. Three major shifting steps are observed in the CH



Fig. 1: ATR-FTIR spectra of; (a) norfloxacin, (b) CH film, (c) CH-NOR0.1 film (d) CH-NOR1.0 film, and (e) CH-NOR5.0 film.



Fig. 2: Tensile strength vs strain-at-break curve of chitosan film (CH) and CH films added with norfloxacin: CH-NOR0.1, CH-NOR1.0 and CH-NOR5.0

film spectrum upon addition of norfloxacin, i.e. shifting of the broad band of -OH stretching (3401.10 cm<sup>-1</sup>), antisymmetric deformation of N-H vibration in NH<sub>a</sub>+ ions (1650.45 cm<sup>-1</sup>) and C-H bending functional group (1421 cm<sup>-1</sup>). The broad band of -OH stretching in CH films at 3401.10 cm<sup>-1</sup>shifted upon addition of norfloxacin, i.e. CH-NOR0.1, CH-NOR1.0 and CH-NOR5.0 at 3293.74 cm<sup>-1</sup>, 3294.13 cm<sup>-1</sup> and 3306.52 cm<sup>-1</sup>, respectively. According to Pierog and co-workers, the shifting occurred within this range indicates the formation of hydrogen bonding from the interaction of O-H (norfloxacin) and N-H (chitosan) stretching vibrations<sup>21</sup>. The shifting of 1650.45 cm<sup>-1</sup> peak of CH film was also observed in CH-NOR films ranging from 1624-1641 cm<sup>-1</sup> which was assigned to antisymmetric deformation of N-H vibration in NH,+ ions. Meanwhile, the C-H bending functional group of CH film at 1421.89 cm<sup>-1</sup> shifted to almost similar wavelength at 1411 cm<sup>-1</sup> for CH-NOR01, CH-NOR1.0 and CH-NOR5.0 films. Other than that, the inclusion of norfloxacin also caused the carbonyl group (C=O) at 1740.44 cm<sup>-1</sup> in CH film disappear in all CH-NOR films. This could indicate that carbonyl group (C=O) of chitosan, i.e. amide group, is possibly involved in the interaction between chitosan and norfloxacin through hydrogen bonding.

# **Mechanical properties**

The mechanical properties of the CH film with inclusion of norfloxacin are shown in Fig. 2 and summarized in Table 1. The addition of norfloxacin into CH resulted in increased strain-at-break ( $\gamma$ ) at a cost of decreased tensile strength (TS) of the film, whereby CH-NOR5.0 film exhibited the  $\gamma$  at 80 ± 1 % and 9 ± 1 MPa for TS (Table 1). For comparison, the  $\gamma$  of CH-NOR0.1 film (lowest concentration of norfloxacin) was recorded at 71 ± 4 % and 15 ± 3 MPa for TS. Nevertheless, all the CH films with norfloxacin show higher mechanical properties (TS, YM, T and  $\gamma$ ) than CH free-standing film (Table 1).

The improvement in the mechanical properties of the CH-NOR films could result from hydrogen bonding between CH with norfloxacin as discussed in ATR-FTIR results. Previous studies have also reported that the increased strain-at-break in polymer-synthetic polymers composites can be attributed to the formation of hydrogen bonding between the chitosan and poly( $\epsilon$ -caprolactone)<sup>22</sup>. Besides that, we could also suggest that the

mechanical reinforcement in composite materials is due to the good film forming property between the polymers used<sup>23</sup>.

#### Swelling and water vapor transmission rates

The swelling results show that the addition of norfloxacin to the CH film resulted in increasing of the water uptake (Table 1). CH films absorbed 292 ± 24 % in phosphate buffer solution (pH 7.2) and increased to 524 ± 65 % for CH-NOR1.0 films. For CH free-standing film, it has been suggested that the swelling of CH materials is a result of electrostatic repulsion between CH chains<sup>24</sup>. With the addition of norfloxacin, the electrostatic repulsion between CH chains has been perturbed and new bonding between CH and norfloxacin caused the swelling value has increased. Similar results have been observed for water swelling of chitosan sponge with norfloxacin in which the swelling ratio was increased by increasing the norfloxacin content<sup>17</sup>. Nevertheless, the swelling degree has decreased for CH-NOR5.0 films probably due to the higher compactness in CH film (increased crosslinking by norfloxacin) thus hindering the water absorption and permeability of the film<sup>25</sup>. In higher crosslinked/ polymer ratio, the crosslinking density increased and eventually reduced the swelling or water uptake of the films significantly.

Swelling percentage and WVTR values obtained in this particular study are correlated due to the fact that both properties exhibit affinity of the film towards water molecule. Water vapor transmission rates (WVTR) values of the CH-NOR films are shown in Table 1. The WVTR value of the CH film was recorded at 1682  $\pm$  170 g m<sup>-2</sup> d<sup>-1</sup> and inclusion of norfloxacin increased the WVTR values to 1883  $\pm$  43 g m<sup>-2</sup> d<sup>-1</sup> for CH-NOR0.1 film, followed by CH-

NOR1.0 at 1916 ± 78 g m<sup>-2</sup> d<sup>-1</sup>. For CH-NOR5.0 film, the WVTR value was decreased to 1795 ± 64 g m<sup>-2</sup> d<sup>-1</sup> due to higher compactness in CH film<sup>26</sup>. These values (1682 – 1916 g m<sup>-2</sup> d<sup>-1</sup>) are within the range of 8 commercially available wound dressing materials from 90 to 2893 g m<sup>-2</sup> d<sup>-127</sup>. For instance, the optimum WVTR value is important since both moisture and oxygen are very quintessential during wound healing. For chitosan films, the WVTR values are affected by several factors such as deacetylation degree and molecular weight of chitosan, film thickness, temperature and relative humidity of measuring condition<sup>28</sup>.

#### Cell Cytotoxicity

The cell's viability of CH-NOR films stained with Calcein-AM on human dermal fibroblast cell (CRL2522, ATCC) and incubated for 24 h, 48 h and 72 h is shown in Fig. 3. The CRL2522 cells adhering on CH film changed their morphology from spherical to elongated, which is typical for fibroblast cells (Fig. 3[d-f]). Previous study has suggested that the adherence of fibroblast cells on CH film is a result of an electrostatic interaction between positively charged CH chains and negatively charged fibroblast cell membrane<sup>29</sup>. The attachment and growth of CRL2522 cell on CH films are in agreement with previous studies examined against other fibroblast cells<sup>30</sup>.

The addition of norfloxacin to CH films generally promotes the cell growth after being incubated for 24 h. For instance, fluorescence imaging shows that the cells on CH-NOR films is viable (Fig. 3 [g, j, m]). However, the degree of fluorescence observed for cells incubated for 72 hours especially on CH-NOR5.0 films gradually decreased which could possibly indicate that the cells

Table 1: Summary of the tensile strength (TS), Young's modulus (YM), toughness (T), strain-at-break (γ), swelling and water vapor transmission rates (WVTRs) of chitosan films with norfloxacin.

| Sample    | TS     | YM      | T  | γ          | Swelling | WVTR                                 |
|-----------|--------|---------|--|------------|----------|--------------------------------------|
|           | (MPa)  | (MPa)   | (J g <sup>-1</sup> )   | <b>(%)</b> | (%)      | (g m <sup>-2</sup> d <sup>-1</sup> ) |
| CH        | 7 ± 1  | 28 ± 3  | $\begin{array}{c} 1.0 \pm 0.01 \\ 2.2 \pm 0.01 \\ 2.5 \pm 0.9 \\ 1.1 \pm 0.14 \end{array}$ | 71 ± 6     | 292 ± 24 | 1682 ± 170                           |
| CH-NOR0.1 | 18 ± 3 | 48 ± 12 |  | 75 ± 4     | 320 ± 21 | 1883 ± 43                            |
| CH-NOR1.0 | 17 ± 6 | 65 ± 11 |  | 70 ± 5     | 524 ± 65 | 1916 ± 78                            |
| CH-NOR5.0 | 8 ± 1  | 29 ± 2  |  | 82 ± 1     | 287 ± 16 | 1795 ± 64                            |

are dying (Fig. 3 [i, l, o]). To quantify the cell growth on CH-NOR films, cell proliferation was carried out by using CellTiter 96 aqueous one solution assay. The cell proliferation results clearly show that the inclusion of norfloxacin significantly affected the cell growth (Fig. 3 [p]). For example, CH-NOR0.1 film



Fig. 3: Fluorescence microscope images of the cell viability on the (a-c) tissue culture polystyrene plate (TCPP), (d-f) CH film, (g-i) CH-NOR0.1 film, (j-l) CH-NOR1.0 film, (m-o) CH-NOR5.0 film and (p) cell proliferation of CH film and CH-NOR0.1, CH-NOR1.0 and CH-NOR5.0 films cultured in the medium seeded with human skin fibroblast cells (CRL2522) for 24 h, 48 h and 72 h. Scale bars represent 100 μm.



Fig. 4: Qualitative antibacterial property of chitosan film incorporated norfloxacinagaints (a) *Staphylococcus aureus*, (b) *Bacillus cereus*, (c) *Escherichia coli* and (d *Klebsiella pneumoniae*. The chitosan films were cut into 6 mm diameter and placed on Muller Hinton agar and labeled as follow; A) Penicillin disc, B) CH film, C) CH-NOR0.1 film, D) CH-NO1.0 film, and E) CH-NOR5.0 film.

recorded 3150 cells/well after incubated for 24 h and decreased to 1480 cells/well after incubation for 72 h. The same reduction of cell growth was observed for CH-NOR1.0 films in which the cell number was recorded at 1630 cells/well (almost similar reading for CH-NOR0.1) after cultured for 72 h. By adding a higher amount of norfloxacin (0.23 mg/mL) into CH film (CH-NOR5.0), the cell growths significantly decreased after being incubated for 72 h. The cell proliferation results are correlated with the limited of fluorescence degree observed on CH-NOR5.0 film.

Limited number of studies have been reported on the influence of norfloxacin to the cell growth. For example, by doing in-vivo test, a group of researcher discovered that chitosan nanocapsules encapsulated with norfloxacin (5 mg/mL) demonstrated an extremely low toxicity effect by examining the histopathological of different organs in rat<sup>31</sup>. In addition to that, ciprofloxacin has a direct effect to fibroblasts, where the exposure to this drug reduced proliferation of three fibroblasts tested<sup>32</sup>. Besides the possible toxicity induces by norfloxacin, a number of studies also reported the influence of physic-chemistry of the material's surface toward biological responses of viable cells such as hydrophilicity and hydrophobicity of materials<sup>33</sup>. Our results show that the swelling behavior of CH-NOR1.0 films exhibit optimum water uptake at 524 ± 65% as compared to its counterparts. This optimum swelling value could contribute to the moderately wettable substrate and therefore increase the adsorption of serum proteins which eventually enhances cell attachment, spreading and adhesion<sup>34</sup>. This behavior is in agreement with the cell proliferation results of CH-NOR1.0 films in which the substrate shown optimum cell number (3990 cell/well) as compared to other CH-NOR films.

#### Antibacterial Study

The antibacterial activity of the CH-NOR films was quantified by a disk method as shown in Fig. 4 and summarized in Table 2. It was observed that CH film exhibited inhibition against *E. coli* only with a diameter of  $7.7 \pm 0.6$  mm. In general, chitosan has been reported to show strong inhibition towards *E. coli*, but differs with several factors such as molecular weight. Previous study on the bactericidal activity of chitosan against *E. coli* has shown that

| Sample          | Diameter of inhibition zone (mm) |                |                     |                          |  |  |  |
|-----------------|----------------------------------|----------------|---------------------|--------------------------|--|--|--|
|                 | Staphylococcus<br>aureus         | Bacilluscereus | Escherichia<br>Coli | Klebsiella<br>pneumoniae |  |  |  |
| Penicillin disc | 14.0 ± 1.7                       | 11.7± 1.53     | 8.3 ± 0.6           | $6.7 \pm 0.6$            |  |  |  |
| СН              | -                                | -              | $7.7 \pm 0.6$       | -                        |  |  |  |
| CH-NOR0.1       | $13.6 \pm 0.6$                   | 12.3 ± 1.5     | 28.7 ± 1.2          | 18.0 ± 2.6               |  |  |  |
| CH-NOR1.0       | 31.3 ± 1.2                       | $22.7 \pm 0.6$ | 34.7 ± 1.2          | 24.0 ± 1.0               |  |  |  |
| CH-NOR5.0       | 35.3 ± 1.2                       | 28.0 ± 1.0     | 36.7 ± 2.3          | 29.3 ± 2.1               |  |  |  |

 Table 2: Inhibition zone area as the indication of antibacterial properties of the chitosan films incorporated norfloxacin against Staphylococcus aureus, Bacillus cereus, Escherichia coli and Klebsiella pneumoniae.

chitosan caused lysis and cytoplasmic membrane disruption in *E. coli* observed via ultra-structural analysis using TEM<sup>35</sup>.The similar study also suggested that the electrostatic interaction between  $-NH_3^+$  groups of chitosan and the negatively charged phospholipids component (carbonyl and phosphoryl groups) of the cell membrane eventually brought about damage to the bacterial cell membrane<sup>36</sup>. Other study has also reported that the release of protonate glucosamine (due to the protonation of amine group) from the chitosan film could contribute to the inhibition of bacterial growth<sup>37</sup>.

With the addition of norfloxacin to the CH films, the inhibition zones are directly proportional to the amount of norfloxacin added (Table 2). For example, CH-NOR5.0 films show the highest inhibition zone to all microbes tested, i.e. 35.3 ± 1.2 mm, 28.0 ± 1 mm, 36.7 ± 2.3 mm, and 29.3 ± 2.1 mm for Staphylococcus aureus, Bacillus cereus, Escherichia coli and Klebsiella pneumoniae, respectively. The inhibition of bacterial deoxyribonucleic acid (DNA) gyrase and topoisomerase IV gave rise to bactericidal effects of fluoroquinolones antibiotic<sup>38</sup>. A few studies have been reported that norfloxacin is more effective as an antibacterial agent against Gram negative bacteria (Escherichia coli and Klebsiella pneumoniae) than Gram-positive bacteria due to the presence of fluorine atom at 6th position and piperazine moiety in norfloxacin molecular structure<sup>39</sup>. Penicillin on the other hand, is more effective against wide spectrums of Gram-positive bacteria. Almost all strains of Staphylococcus aureus are susceptible to Penicillin<sup>40</sup> and the same trend was observed in our study. From the data tabulated in Table 2, the inhibition zone of Penicillin on Staphylococcus aureus and Bacillus cereus plates are bigger than those of Escherichia coli and Klebsiella pneumoniae. It can be deduced that, Penicillin is a more powerful antibacterial agent in combating the growth of Gram positive bacteria due to the fact that this antibiotic kills bacteria by inhibiting the proteins which crosslinks peptidoglycans in the cell wall<sup>41</sup>. Besides that, gram positive bacteria like Staphylococcus aureus and Bacillus cereus have no additional layer outside the cell wall, hence causing the bacterium to be susceptible to the attack of Penicillin<sup>42</sup>. Escherichia coli and Klebsiella pneumoniae on the other hand, are Gram negative bacteria which have lipopolysaccharide and protein layer surrounding the peptidoglycan layer of its cell wall, hindering Penicillin from attacking it<sup>43</sup>.

## CONCLUSIONS

The chitosan film with norfloxacin (CH-NOR) has been successfully prepared. Addition of norfloxacin into CH film increased the strain-atbreak to 80  $\pm$  1 % than CH film at 69  $\pm$  6 % at a cost of decreased the tensile strength. Swelling behavior of the CH-NOR films are increased and reached optimum at 524 ± 65 %, while water vapor transmission rates of all films are within the range of commercial dressings (1682-1916 g m<sup>-2</sup> d<sup>-1</sup>). The in-vitro cell study shows norfloxacin in CH film perturbed the cell growth at higher concentration (0.23 mg/mL) and longer incubation (72 h). However, inclusion of norfloxacin at higher amount significantly improved the antibacterial activity of CH film against Gram positive (S. aureas, B. cereus) and Gram negative (E. coli, K. pneumoniae).

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# REFERENCES

- Zhang, D.; Zhou, W.; Wei, B.; Wang, X.; Tang, R.; Nie, J.; Wang, J. *Carbohydrate polymers* 2015, *125*, 189-199.
- Galli, C.; Parisi, L.; Elviri, L.; Bianchera, A.; Smerieri, A.; Lagonegro, P.; Lumetti, S.; Manfredi, E.; Bettini, R.; Macaluso, G. *Biomedical Materials* 2016,11, 015004.
- Xu, J.; Strandman, S.; Zhu, J. X.; Barralet, J.; Cerruti, M. *Biomaterials* 2015,37, 395-404.
- Behl, G.; Iqbal, J.; O'Reilly, N. J.; McLoughlin, P.; Fitzhenry, L. *Pharmaceutical research* 2016, 1-11.
- Karthik, R.; Manigandan, V.; Saravanan, R.; Rajesh, R. P.; Chandrika, B. Int. J. Biol. Macromol. 2016,84, 319-328.
- Azuma, K.; Osaki, T.; Minami, S.; Okamoto, Y. *Journal of functional biomaterials* 2015,6, 33-49.
- 7. Jayakumar, R.; Prabaharan, M.; Sudheesh Kumar, P.T.; Nair, S.V.; Tamura, H. *Biotechnol. Adv.* **2011**,*29*, 322-337.
- Sezer, A. D.; Hatipoglu, F.; Cevher, E.; Oðurtan, Z.; Bas, A. L.; Akbuða, J. AAPS PharmSciTech 2007,8, E94-E101.
- Noel, S. P.; Courtney, H.; Bumgardner, J. D.; Haggard, W. O. *Clinical Orthopaedics and Related Research* 2008,466, 1377-1382.
- 10. Wang, Q.; Dong, Z.; Du, Y.; Kennedy, J. F. *Carbohydrate polymers* **2007**,*69*, 336-343.
- Wang, L.-C.; Chen, X.-G.; Zhong, D.-Y.; Xu, Q.-C. Journal of Materials Science: Materials in Medicine 2007, 18, 1125-1133.
- 12. Garrison, M. W. *Diagnostic Microbiology and* Infectious Disease **2006**,*54*, 51-56.
- Santoro, M. I. R. M.; Kassab, N. M.; Singh, A. K.; Kedor-Hackmam, E. R. M. Journal of Pharmaceutical and Biomedical Analysis 2006,40, 179-184.
- Hadimeri, H.; Almroth, G.; Cederbrant, K.; Eneström, S.; Hultman, P.; Lindell, Å. Scandinavian journal of urology and

nephrology **1997**,*31*, 481-485.

- Lindgren, P.K.; Marcusson, L.L.; Sandvang, D.; Frimodt-Møller, N.; Hughes, D. Antimicrobial Agents and Chemotherapy 2005,49, 2343-2351.
- Campillo, B.; Dupeyron, C.; Richardet, J.-P.; Mangeney, N.; Leluan, G. *Clinical infectious diseases* 1998,26, 1066-1070.
- Denkba<sup>o</sup>, E. B.; Öztürk, E.; Özdemir, N.; Keçeci, K.; Agalar, C. *J. Biomater. Appl.* 2004, *18*, 291-303.
- XUE, C.-g.; TONG, C.-y.; XIAO, S.-y.; WANG, B.; YU, D.-m.; TANG, D.-y.; LIU, X.-m. Journal of Central South University (Science and Technology) 2008,3, 013.
- Dua, K.; Ramana, M. V.; Sara, U. V. S.; Agrawal, D. K.; Pabreja, K.; Chakravarthi, S. *Eplasty* 2010, *10*, e44.
- Mishra, R.; Majeed, A.; Banthia, A. International Journal of Plastics Technology 2011, 15, 82-95.
- Pierog, M.; Gierszewska-Dru¿yñska, M.; Ostrowska-Czubenko, J. Progress on Chemistry and Application of Chitin and its Derivatives. Polish Chitin Society, £ódŸ 2009.75, 82.
- Sarasam, A.; Madihally, S. V. *Biomaterials* 2005, 26, 5500-5508.
- 23. Nagahama, H.; Maeda, H.; Kashiki, T.; Jayakumar, R.; Furuike, T.; Tamura, H. *Carbohydrate Polymers* **2009**,*76*, 255-260.
- Qu, X.; Wirsén, A.; Albertsson, A. C. *Polymer* 2000,41, 4589-4598.
- 25. Varshosaz, J.; Koopaie, N. *Iranian Polymer Journal* **2002**, *11*, 123-131.
- 26. Fu, S.-Y.; Feng, X.-Q.; Lauke, B.; Mai, Y.-W. *Composites Part B: Engineering* **2008**,*39*, 933-961.
- 27. Wu, P.; Fisher, A.; Foo, P.; Queen, D.; Gaylor, J. *Biomaterials* **1995**, *16*, 171-175.
- 28. Srinivasa, P.; Ramesh, M.; Kumar, K.;

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Tharanathan, R. *Journal of Food Engineering* **2004**,*63*, 79-85.

- Ding, Z.; Chen, J.; Gao, S.; Chang, J.; Zhang, J.; Kang, E. T. *Biomaterials* 2004,25, 1059-1067.
- Howling, G. I.; Dettmar, P. W.; Goddard, P. A.; Hampson, F. C.; Dornish, M.; Wood, E. J. Biomaterials 2001,22, 2959-2966;
- Raþã, D.; Popa, M.; Chailan, J.-F.; Zamfir, C.; Peptu, C. *Journal of Nanoparticle Research* 2014, 16, 1-10.
- Williams, R. J.; Attia, E.; Wickiewicz, T. L.; Hannafin, J. A. *The American journal of sports medicine* 2000,28, 364-369.
- Ruardy, T. G.; Moorlag, H. E.; Schakenraad, J. M.; Van Der Mei, H. C.; Busscher, H. J. *Journal* of Colloid and Interface Science 1997,188, 209-217.
- Van Wachem, P.; Beugeling, T.; Feijen, J.; Bantjes, A.; Detmers, J.; Van Aken, W. Biomaterials 1985,6, 403-408.
- 35. Li, X.-f.; Feng, X.-q.; Yang, S.; Fu, G.-q.;

Wang, T.-p.; Su, Z.-x. *Carbohydrate Polymers* **2010**, *79*, 493-499.

- Liu, H.; Du, Y.; Wang, X.; Sun, L. International journal of food microbiology 2004,95, 147-155.
- Fernandez-Saiz, P.; Lagaron, J.; Ocio, M. Food Hydrocolloids 2009,23, 913-921.
- Gürbay, A.; Garrel, C.; Osman, M.; Richard, M.; Favier, A.; Hincal, F. *Human & experimental toxicology* 2002,21, 635-641.
- 39. Sharma, P. C.; Saneja, A.; Jain, S. *Int J Chem Sci* **2008**,*6*, 1702-1713.
- 40. Rice, L. B. *American journal of infection control* **2006**,*34*, S11-S19.
- 41. Fair, R. J.; Tor, Y. *Perspectives in medicinal chemistry* **2014**,*6*, 25.
- Feng, Q.; Wu, J.; Chen, G.; Cui, F.; Kim, T.; Kim, J. *Journal of biomedical materials* research 2000,52, 662-668.
- 43. Beveridge, T. J. *J. Bacteriol.* **1999**, *181*, 4725-4733.